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Uptake of calcium and silicon released from calcium silicate-based endodontic materials into root canal dentine

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Abstract

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Aim To compare Biodentine and White ProRoot mineral trioxide aggregate (MTA) with regard to Ca and Si uptake by adjacent root canal dentine in the presence of phosphate-buffered saline (PBS).

Methodology Root canals of bovine incisor root segments were instrumented, filled with either Biodentine or MTA (n = 20 each) and then immersed in Ca-and Mg-free PBS for 1, 7, 30 or 90 days (n = 5 each). Unfilled, unimmersed dentine specimens (n = 5) served as controls. The specimens were sectioned longitudinally, and the ultrastructure of the dentinematerial interface and the elemental composition/ distribution in the material–adjacent dentine were analysed using a wavelength-dispersive X-ray spectroscopy electron probe microanalyser with image

observation function. Data were statistically analyzed using one-way ANOVA and Tukey's honestly significant difference test or the Mann–Whitney *U*-test.

Results Along the material–dentine interface, both materials formed a tag-like structure that was composed of either Ca- and P-rich crystalline deposits or the material itself. The width of a Ca- and Si-rich layer detected along the dentine layer of the material–dentine interface showed increases over time. The Ca- and Si-rich layer width was significantly larger (P < 0.05) in Biodentine than MTA at 30 and 90 days.

Conclusions Both Biodentine and MTA caused the uptake of Ca and Si in the adjacent root canal dentine in the presence of PBS. The dentine element uptake was more prominent for Biodentine than MTA.

Keywords: bioactivity, Biodentine, calcium, element uptake in dentine, mineral trioxide aggregate, silicon.

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Introduction

Mineral trioxide aggregate (MTA) is a calcium silicate– based endodontic material that has been developed by modification of Portland cement (Camilleri *et al.* 2005, Dammaschke *et al.* 2005). A number of laboratory and *in vivo* studies have demonstrated that MTA possesses excellent biocompatibility and sealing ability (Torabinejad & Parirokh 2010); thus, it is currently considered the most promising material for various treatments such as root-end filling (Chong *et al.* 2003, Saunders 2008, Baek *et al.* 2010), direct pulp capping (Nair *et al.* 2008, Okiji & Yoshiba 2009, Mente *et al.* 2010), perforation repair (Main *et al.* 2004) and apical barrier for teeth with necrotic pulps and open apexes (Simon *et al.* 2007).

The bioactivity of MTA has been attributed to its ability to produce surface apatite crystals when in contact with phosphate solutions such as phosphatebuffered saline (PBS) (Sarkar *et al.* 2005, Bozeman *et al.* 2006, Tay *et al.* 2007, Reyes-Carmona *et al.* 2009, Gandolfi *et al.* 2010, Han *et al.* 2010). The crystalline precipitates are formed through interaction of Ca and OH ions released from set MTA (Camilleri 2008a) with phosphates and have been identified as

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calcium-deficient B-type carbonated apatite precipitates produced via an amorphous calcium phosphate phase (Tay *et al.* 2007). Moreover, apatite crystal formation has also been demonstrated along the MTA–dentine interface and within the interfacial dentine (Sarkar *et al.* 2005, Reyes-Carmona *et al.* 2009, 2010). These findings lead to the notion that apatite formation contributes to leakage reduction not only by filling the gap along the interface but also via dentine interactions such as intrafibrillar apatite deposition. This is supported by the finding that immersion in PBS decreases marginal leakage of MTA apical plugs (Martin *et al.* 2007).

Several new calcium silicate-based materials have recently been developed (Asgary et al. 2008, Camilleri 2008b, Gandolfi et al. 2008, Gomes-Filho et al. 2009), aiming to improve some MTA drawbacks such as its difficult handling property (Johnson 1999) and long setting time (Torabinejad et al. 1995, Dammaschke et al. 2005). Biodentine (Septodont, Saint Maur des Fossés, France) is amongst these materials and is claimed to be used as a dentine restorative material in addition to endodontic indications similar to those of MTA. Biodentine powder is mainly composed of tricalcium silicate, calcium carbonate and zirconium oxide as the radio-pacifier, whilst Biodentine liquid contains calcium chloride as the setting accelerator and waterreducing agent (Laurent et al. 2008). Biodentine shows apatite formation after immersion in phosphate solution (Goldberg et al. 2009), indicative of its bioactivity.

Dentine may uptake several elements released from bioactive materials, and such a phenomenon may cause chemical and structural dentine modification resulting in acquisition of higher acid resistance and remineralisation (Hotta *et al.* 2001). The element incorporation by adjacent dentine may also be regarded as an indicator of the material's bioactivity. However, information is limited regarding how the elements released from different calcium silicate–based materials are incorporated in the dentine in contact with these materials. Thus, the aim of this study was to compare Biodentine and MTA with regard to Ca and Si uptake by the adjacent root canal dentine in the presence of PBS.

Material and methods

This study used two commercially available calcium silicate cements: BiodentineTM (Septodont, Saint-Maurdes Fosses, France, Lot: 48032) and White ProRoot MTA (MTA; Dentsply Tulsa Dental, Tulsa, OK, USA, Lot: 08003395).

Sample preparation

Bovine incisors obtained from a Japanese slaughterhouse were used throughout this study. The study exerted no influence on the animal's fate at any stage. Bovine incisor roots were sectioned at the coronal (approximately 4 mm below the cementoenamel junction) and apical (approximately 8 mm above the apex) levels, and the resulting root segments were further ground to 4-mm lengths. The canals of these cylindrical specimens were instrumented using a size 140 Kfile (Mani, Tochigi, Japan) under copious irrigation by using 3% sodium hypochlorite (Neo Cleaner; Neo Dental, Tokyo, Japan). The canals were then irrigated with 18% ethylenediaminetetraacetic acid (Ultradent, South Jordan, UT, USA) followed by 3% sodium hypochlorite for 1 min each, washed immediately with purified water and dried using absorbent paper points (VDW, Munich, Germany). These specimens were assigned to one of three groups: Biodentine (n = 20): MTA (n = 20); and unfilled, unimmersed dentine specimens (n = 5).

Biodentine and MTA were mixed according to the manufacturers' instructions and inserted into the prepared root canal specimens by using an appropriate root canal condenser (YDM, Tokyo, Japan). The specimens were stored for 2 h at 100% relative humidity to allow initial setting of the materials and then immersed individually in plastic vials containing 20 mL of Caand Mg-free PBS (136.4 mmol L⁻¹ NaCl, 2.7 mmol L⁻¹ KCl, 8.2 mmol L⁻¹ NaH₂PO₄ and 1.25 mmol L⁻¹ KH₂PO₄ in 1000 mL of distilled water; pH 7.4) for 1, 7, 30 or 90 days (n = 5, in each period). The immersion solution was replaced every 7 days for the long-term immersion specimens.

After the given periods of time, the specimens were sectioned longitudinally into two symmetrical pieces. One of the two halves was processed for morphological observation, element mapping and chemical analysis along the dentine–material interface, whilst the other half was saved for scanning of the elemental incorporation depth within the root canal dentine as described later.

Morphological and element analysis

The specimens were mounted on aluminium stubs, sputter-coated with a 300-Å-thick gold layer with an ion coater (IC-50; Shimadzu, Kyoto, Japan) and analysed using a wavelength-dispersive X-ray spectroscopy electron probe microanalyser with an image observation function (SEM-EPMA, EPMA1601; Shimadzu, Kyoto, Japan).

For the morphological observation, the outermost dentine layers of the dentine–material interface were analysed under SEM-EPMA at an accelerating voltage of 15 kV.

Chemical component bulk analysis and element mapping was carried out using SEM-EPMA for the outermost dentine area (60–70 μ m away from the interface). The incorporation depths of Ca and Si into the dentine were measured using the elemental line scan from the interface to the direction of inner dentine in the range of 300–500 μ m.

Statistical analysis

Data obtained were recorded and analysed using oneway ANOVA and Tukey's honestly significant difference (HSD) test or the Mann–Whitney *U*-test with a significance level of 5%.

Results

Scanning electron microscopy (SEM) analysis revealed the presence of an 'interfacial layer,' which was identified as a 'brighter area' under the back-scattered electron imaging on the longer PBS immersion specimen (Figs 1 and 2) and a tag-like structure within the dentinal tubules along the dentine–material interface (Fig. 1). Part of the brighter area on the interfacial layer and the tag-like structure was subjected to chemical composition analysis and was revealed to be involved in the Ca and Si increases. The interfacial layer appears brighter in the longer period PBS immersion specimens (Figs 1 and 2).

Results of the bulk chemical analyses on the interfacial dentine layer over the 90-day PBS immersion period are shown in Table 1 (Biodentine) and Table 2 (MTA). In control (unfilled) dentine specimens, Ca, O, P and C were detected as the principal elemental dentine components. Following PBS immersion, the relative concentration of these elements showed some changes, most notably increases in Si concentration and Ca/P ratio. In both the Biodentine and MTA specimens, the Ca/P ratio showed significant increases at all the time points compared with those of the control (P < 0.05, one-way ANOVA and Tukey's HSD test). Moreover, Si percentages increased in both Biodentine and MTA with time, although Si was not detected in the control dentine specimens.

Element mapping revealed that Ca- and Si-rich dentine areas were observed along the dentine–material interface (Fig. 2). On the other hand, as shown in Table 3, the Biodentine and MTA specimens showed increased incorporation depths as the immersion periods increased. The Ca depth was constantly larger than the Si depth. Moreover, Biodentine specimens constantly showed larger values versus the corresponding MTA specimen values, and significant differences were noted at all time points for Ca and only at 30 and 90 days for Si (P < 0.05, Mann–Whitney U-test).

Discussion

The present results demonstrated the uptake of Ca and Si in the dentine in contact with both Biodentine and MTA occurred following PBS immersion. This may represent the biomineralisation ability of these calcium silicate materials promoted by the interaction with dentine in the presence of phosphate-containing solutions (Sarkar *et al.* 2005, Reyes-Carmona *et al.* 2009, 2010). Ca and Si uptake most probably causes chemical and structural modification of dentine, which may result in higher acid resistance and physical strength.

The present results also demonstrated that Biodentine may have a more prominent biomineralisation ability than MTA, as Biodentine specimens showed wider Ca- and Si-rich dentine areas (Fig. 2) and larger incorporation depths (Table 3) than MTA revealed by element mapping and line-scan analysis, respectively.

Figure 1 Representative SEM micrographs of the Biodentine–dentine interface after 24 h (a) and 30 days (b) of phosphate-buffered saline immersion. Insets show lower magnification images and boxed areas depict the areas enlarged. TS: tag-like structure. (a) Bar, 10μ m; in inset, 100μ m. (b) Bar, 5μ m; in inset, 50μ m.





Figure 2 SEM micrographs (a, d) and mapping images for Ca (b, e) and Si (c, f) obtained by SEM-EPMA. Biodentine (BD)–dentine (a, b, c) and mineral trioxide aggregate (MTA)–dentine (d, e, f) interfacial areas of representative specimens after 30-day phosphate-buffered saline immersion. TS: tag-like structure. Dotted lines show the approximate interface position (bar, 20 μ m; grey and colour bars, X-ray strength).

| Elements | Control | Phosphate-buffered saline immersion | | | |
|----------|------------|-------------------------------------|------------|------------|------------|
| | | 24 h | 7 days | 30 days | 90 days |
| Са | 32.3 (0.3) | 42.8 (4.1) | 43.9 (3.6) | 43.7 (4.3) | 44.9 (7.2) |
| 0 | 26.8 (0.3) | 22.9 (4.5) | 24.4 (4.6) | 23.9 (5.4) | 22.1 (2.1) |
| Р | 26.5 (1.0) | 22.7 (3.1) | 21.1 (3.2) | 21.7 (3.3) | 21.9 (3.3) |
| С | 12.1 (1.0) | 9.0 (2.4) | 7.4 (1.4) | 7.0 (1.8) | 6.3 (1.5) |
| Si | 0.0 (0.0) | 0.7 (0.2) | 1.2 (0.2) | 1.7 (0.2) | 3.2 (0.2) |
| Ca/P | 1.2 (0.1)a | 1.9 (0.1)b | 2.1 (0.2)b | 2.0 (0.1)b | 2.1 (0.2)k |

 Table 1
 Principal composition of the interfacial dentine layer of the Biodentine group (atomic %)

Mean (SD), n = 5.

Mean values followed by different letters (Ca/P) are significantly different (P < 0.05).

| Elements | Control | Phosphate-buffered saline immersion | | | |
|----------|------------|-------------------------------------|------------|------------|------------|
| | | 24 h | 7 days | 30 days | 90 days |
| Са | 32.3 (0.3) | 36.3 (6.0) | 37.1 (6.2) | 37.9 (6.4) | 40.2 (5.6) |
| 0 | 26.8 (0.3) | 27.6 (5.9) | 28.8 (4.1) | 25.2 (1.7) | 24.7 (5.0) |
| Р | 26.5 (1.0) | 23.0 (3.3) | 22.6 (3.2) | 23.1 (4.4) | 23.1 (3.5) |
| С | 12.1 (1.0) | 8.9 (0.4) | 7.1 (1.0) | 9.8 (1.4) | 7.5 (1.1) |
| Si | 0.0 (0.0) | 1.0 (0.2) | 0.8 (0.1) | 1.0 (0.7) | 1.2 (0.2) |
| Ca/P | 1.2 (0.1)a | 1.6 (0.3)ab | 1.7 (0.2)b | 1.7 (0.2)b | 1.8 (0.2)b |

Table 2 Principal composition of theinterfacial dentine layer of the mineraltrioxide aggregate group (atomic %)

Mean (SD), n = 5.

Mean values followed by different letters (Ca/P) are significantly different (P < 0.05).

This could be because of the amount of Ca and Si dissolution that could be larger in Biodentine than in MTA.

Chemical analysis of the interfacial dentine layer confirmed increased Ca levels and Ca/P ratios in the Biodentine and MTA specimens. This finding is related Table 3 The incorporation depths of calcium and silicon into the dentine (µm)

| Phosphate-buffered | C | a | Ś | Si |
|--------------------|---------------|---------------|---------------|---------------|
| saline immersion | Biodentine | MTA | Biodentine | MTA |
| 24 h | 66.8 (5.1)a | 14.4 (3.8)b | 17.6 (2.5)a | 13.8 (2.2)a |
| 7 days | 116.8 (10.1)a | 77.8 (13.5)b | 71.2 (10.0)a | 61.0 (8.9)a |
| 30 days | 212.2 (26.4)a | 166.8 (10.1)b | 160.2 (16.1)a | 115.4 (24.0)b |
| 90 days | 296.0 (26.0)a | 206.6 (15.1)b | 275.8 (28.9)a | 171.2 (33.4)b |

Mean (SD), n = 5.

Mean values followed by different letters in the same line of the same element are significantly different (P < 0.05). MTA, mineral trioxide aggregate.

to Ca incorporation. As such, the quality of the interfacial dentine layer appeared to be improved. On the other hand. Si also accumulated in the same area.

The apatite-forming ability of an artificial material in the presence of phosphate solutions ex vivo is regarded as a prerequisite for achieving bonds between the material and living bone (Kokubo & Takadama 2006). It is known that calcium silicate-based ceramic materials commonly exhibit bioactivity to induce bone-like apatite formation (Liu et al. 2008); various calcium silicate-based ceramic materials are reported to show such activity, including Portland cement (Tay et al. 2007, Reyes-Carmona et al. 2009), dicalcium silicate (Gou et al. 2005) and tricalcium silicate (Zhao et al. 2005). Apatite formation on the calcium silicate-based materials may be attributed to the dissolution of portlandite (calcium hydroxide that formed as a result of hydration reactions of calcium silicate materials): this dissolution causes increased pH and Ca2+ ion concentration, which in turn may enhance the supersaturation of phosphate-containing fluid with respect to apatite and, hence, promote precipitation. It has also been described that functional groups, such as Si-OH pre-existing on nanoporous calcium silicate hydrate gel structures formed following hydration reactions, act as nucleation centres for apatite precipitation (Kokubo & Takadama 2006).

Studies on the ultrastructure of the MTA-dentine interface following PBS immersion have demonstrated the formation of a mineral-rich interfacial layer and a tag-like structure extending from the interfacial layer to the dentinal tubules (Sarkar et al. 2005, Reyes-Carmona et al. 2009). Formation of a 'mineral tag' has also been demonstrated in Biodentine-dentine interfaces (Goldberg et al. 2009). The present study confirmed these findings and further demonstrated different taglike structures with different PBS immersion periods in the relative elemental composition (representative example, Fig. 1). This difference may be attributable to the difference in the amount of Ca release between the PBS immersion periods; Biodentine may release a larger amount of Ca and, consequently, produce larger amounts of calcium phosphate precipitates in the PBS environment. Such a property may have positively influenced the formation of the interfacial layer and the tag-like structure.

Formation of the interfacial layer and tag-like structures may be responsible for the good marginal seal of MTA (Torabinejad & Parirokh 2010). This notion is supported by the finding that immersion in PBS decreases marginal leakage of MTA apical plugs (Martin et al. 2007). It has also been reported that immersion of MTA in PBS increases push-out strength (Reves-Carmona et al. 2010), suggesting that the biomineralisation ability confers the material with greater resistance to dislodgement, most likely through the formation of tags, which constitutes micromechanical anchorage. Biodentine is believed to have the potential to exhibit similar characteristics.

This study demonstrated the formation of a Si-rich layer in dentine in contact with Biodentine and MTA. The Si-rich layer was constantly narrower than the Carich layer (Fig. 2), most likely because the amount of Si released from MTA is much smaller than that of Ca (Sarkar et al. 2005, Bozeman et al. 2006, Camilleri 2008a). The precise role of Si in hard tissue metabolism remains unclear, although it is believed to play a role in the early bone calcification process (Carlisle 1970). Si is also known to enhance the rate of new bone growth when released from bioactive materials in vivo (Patel et al. 2002). Moreover, Si is reported to induce remineralisation of demineralised dentine in vitro (Saito et al. 2003). These findings suggest that the release of Si from calcium silicate-based materials may confer additional in vivo bioactivity of these materials.

Conclusions

Both Biodentine and MTA caused the uptake of Ca and Si in the adjacent root canal dentine in the presence of PBS. The elemental uptake into dentine was more prominent for Biodentine than for MTA.

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