



Biological Adaptation to Misfits of Immediately Loaded Fixed Prostheses Following Computer-Guided Surgery

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Abstract

In this clinical report, following computer-guided (3D Procera Software Planning Program, Nobel Biocare, Yorba Linda, CA) placement and immediate provisionalization of 12 dental implants (NobelSpeedy™ Replace, Nobel Biocare), misfits of the prefabricated screw-retained interim prostheses were noted at several implant-abutment junctions. Nevertheless, adaptation of the misfits was observed 10 days later, after the loosened screws were tightened. While a high mean marginal bone loss of 2.1 mm (range: 1.4 to 3.5 mm) was noted, all implants remained osseointegrated at 3-year follow-up.

Immediate loading of implant-supported fixed complete dentures (FCDs) has been documented with high success rates in both the edentulous maxilla and mandible.¹⁻¹³ While immediate loading procedures nullify the 3- to 6-month period of undisturbed implant healing and eliminate the need for removable prostheses, immediate loading remains a technique-sensitive and demanding task, both surgically and restoratively. Recently, computer-guided implant surgery was conceived to coordinate optimum treatment planning and execution, resulting in accurate and minimally invasive surgical procedures.¹⁴⁻¹⁹ The original protocol entailed the conversion of the complete denture into a functionally loaded fixed complete dentures (FCDs) immediately following computer-guided implant surgery.¹³ Recently, others have advocated immediate placement of either a provisional or definitive FCD prefabricated from computer-simulated implant positions.¹⁷⁻²⁰ Although efforts have been made to minimize potential processing errors, the risk of prosthetic misfit is not negligible.^{20,21}

While a small degree of prosthetic misfit on natural dentition can sometimes be mitigated due to the adaptability of the periodontal ligament, such adaptation has not been observed in integrated implants, as they are ankyrotic in nature. This is especially true for screw-retained implant prostheses where the misfit cannot be compensated by the cement space present in the cement-retained implant prosthesis. Although prosthetic misfit has not been shown to result in loss of implant osseointegration,²²⁻²⁷ it is known to introduce undue stress on the implants, screws, prostheses, and surrounding bone, resulting in mechanical complications of the implants and/or implant components, as well as an increase in crestal bone loss.²⁴ Thus, passive fit of implant prosthesis framework remains a goal for biomechanical success, especially in immediate provisionalization situations where excessive forces must be avoided.²⁴

This clinical report demonstrates a situation in which an implant-prosthesis adaptation was noted 10 days following implant placement in the initially misfit, immediately loaded,



Figure 1 Preoperative panoramic radiograph displayed generalized severe alveolar bone loss.

implant-supported FCDs. The implants were placed using computer-guided protocol.

Clinical report

A 45-year-old female patient presented with severely periodontally compromised maxillary and mandibular dentition, which were deemed hopeless (class III complete edentulism according to the Prosthodontic Diagnostic Index²⁸) (Fig 1). While several treatment options were presented, the patient wished to pursue a treatment plan that included implant-supported maxillary and mandibular FCDs following extraction of the remaining dentition. To provide the patient with esthetic and functional convenience, a treatment plan involving computer-guided implant surgery and immediate loading with interim FCDs was proposed and accepted.

After a healing period of 4 months following extractions of the remaining dentition and placement of interim complete dental prostheses, definitive maxillary and mandibular complete dentures were fabricated with the appropriate function, occlusal vertical dimension, and esthetics to serve as a template for the computer-guided implant surgery. After radiopaque markers (Hygenic Temporary Dental Stopping, Coltene/Whaledent Inc., Cuyahoga Falls, OH) were incorporated into the dentures, the patient received a cone beam computed tomography (Newtom 3G, QR SRL, Verona, Italy) using the “double scan” technique. The first scan was made with the patient wearing the complete dentures with the radiopaque markers, while the second scan was performed with the dentures alone in the same orientation as with the first scan.

The Digital Imaging and Communications in Medicine (DICOM) data of the two sets of scans were transferred to the 3D Procera Software Planning program (Nobel Biocare, Yorba Linda, CA) and superimposed to evaluate the osseous architecture in relation to the denture for the planning of the number, length, position, and angulation of the implants. Six implants (NobelSpeedyTM Replace, Nobel Biocare) were planned for each arch.

The data were sent to the milling center for the fabrication of the stereolithographic surgical template (Nobel Biocare). To fabricate the maxillary and mandibular working cast, the implant replicas (Nobel Biocare) were mounted in each of the metal sleeves in the surgical template using guided cylinders

with unigrip pins (Guided Cylinder with Pin UnigripTM NobRpl RP, Nobel Biocare). The anchor pins were then inserted into the anchor pin sleeves and secured with utility wax. A silicone-based material (GI Mask, Coltene/Whaledent Inc.) was applied to the intaglio surface of the surgical template and trimmed to expose the replicas and anchor pins. The working casts were then made with dental die stone plaster (Modern Materials Die-Keen Green, Heraeus Kulzer, Inc., South Bend, IN) and mounted on an articulator for the fabrication of full-arch, screw-retained fixed interim prostheses.

At the surgical appointment, after local anesthetic administration, proper seating of the surgical templates was ascertained. Osteotomies were then made through the guided anchor pin sleeves on the surgical template using the guided twist drill (Guided Twist Drill, 1.5 mm × 20 mm, Nobel Biocare). Guided anchor pins (Nobel Biocare) were then inserted to secure the template for the surgical procedure. Sequential osteotomies were made according to the surgical templates, and six implants (NobelSpeedyTM Replace) were placed with a minimum of 35 Ncm insertion torque in each of the patient’s edentulous arches (Table 1). The implant platforms were placed at the crest, as designed with preoperative computer simulation, and verified by assuring full contact between the implant drivers and the mating surface of the guide sleeves.

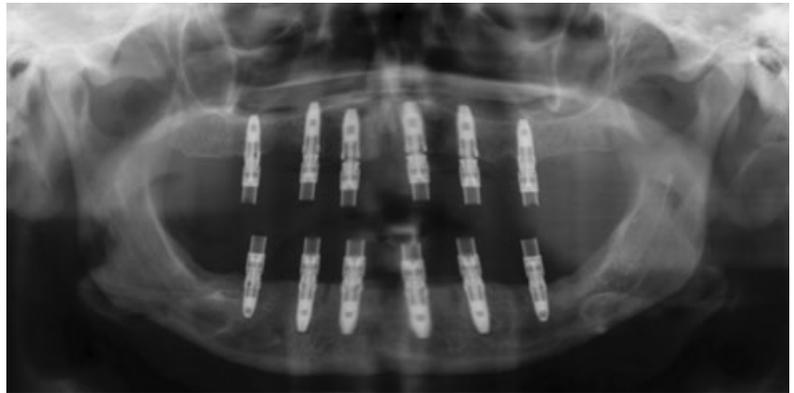
Table 1 Surgical data of the computer-guided surgery

Implant position	Bone quality (I to IV)	Implant diameter (mm)	Implant length (mm)	Last drill diameter (mm)	Insertion torque (Ncm)
4	III	4.0	11.5	3.2	>35
6	II	4.0	13	3.2	>35
7	II	4.0	13	3.2	>35
10	II	4.0	13	3.2	>35
11	II	4.0	13	3.2	>35
13	II	4.0	11.5	3.2	>35
20	II	4.0	10	3.2	>35
22	I	4.0	13	3.2	>35
23	I	4.0	13	3.2	>35
26	I	4.0	13	3.2	>35
27	I	4.0	13	3.2	>35
29	II	4.0	10	3.2	>35

Figure 2 Panoramic radiograph immediately after the placement of maxillary and mandibular provisional fixed complete prostheses. Note the apparent prosthesis misfit at the majority of the implant/abutment interfaces.



Figure 3 After multiple adjustments, although a significant improvement was observed, passive fit was never achieved.



The prefabricated maxillary and mandibular interim prostheses were hand-tightened onto the implants with self-adjustable abutments designed to compensate for up to 0.4 mm of vertical discrepancies (Guided Abutment NobRpl RP, Nobel Biocare). Despite numerous time-consuming attempts to passively seat the prostheses by alternately hand tightening and loosening the prosthetic screws in different order and sequence, radiographic passive fit was not achieved (Figs 2 and 3). Since only minor adjustments were required to achieve a stable centric and eccentric occlusion without interferences, the patient was dismissed with the misfit interim prostheses to have them either sectioned and reconnected or refabricated for passive fit at a subsequent appointment. All prosthetic screws were hand-tightened, and the screw access holes were sealed with poly(vinyl siloxane) material (Exafast™ NDS Heavy body, GC America Inc., Alsip, IL). Appropriate antibiotics and analgesics were prescribed postoperatively. The patient was instructed not to brush the surgical site, but rinse gently with 0.12% chlorhexidine gluconate (Peridex, Procter & Gamble, Cincinnati, OH), and to be on a liquid diet for 2 weeks. A soft diet was recommended for the remaining duration of the implant healing phase (4 months).

Four days after surgery, the patient complained of severe pressure to the maxilla and mandibular implants. Loosening each of the prosthetic screws by a quarter of a turn instantly relieved the pressure. Nevertheless, periapical radiographs and orthopantomogram (Sirona Dental Systems LLC, Charlotte, NC) still showed incomplete seating of the interim prosthe-

ses. Ten days after the surgery, the patient returned with loose mandibular and maxillary prostheses due to the prosthetic screw loosening. All screws were retightened by hand and surprisingly, complete radiographic passive abutment seating was noted (Fig 4).

Six months following implant surgery, despite stability observed in all implants, mean 2.1 mm marginal bone loss (range: 1.4 to 3.5 mm) was noted with sequential standardized periapical radiographs (Fig 5). When assessing marginal bone loss, the implant platform was used as the reference line. Marginal bone loss at the follow-up appointment was defined as the distance from the implant platform to the implant/bone contact point apical to the platform. When the implant/bone contact point was at or coronal to the implant platform, it was considered as 'no change.' The definitive impressions were made using poly(vinyl siloxane) material (Aquasil, Dentsply Caulk, Milford, DE). The screw-retained definitive metal ceramic profile maxillary and mandibular FCDs were seated and torqued to 35 Ncm. Periapical radiographs and orthopantomogram (iCAT) were used to verify the fit of the prostheses (Fig 6).

Discussion

It has been postulated that progressive chronic marginal infection (peri-implantitis) and excessive loading are factors contributing to osseointegrated implant failures.²⁹ A gap at the implant/abutment interface resulting from implant framework misfit could harbor a large quantity of microorganisms as well

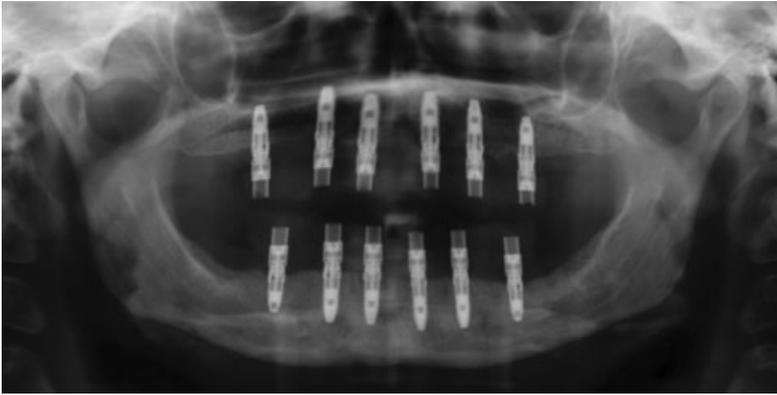


Figure 4 Ten days after the surgery, framework fit was achieved with hand tightening after the patient complained of loose maxillary and mandibular prostheses.



Figure 5 Periapical radiograph 6 months after the surgery showed significant peri-implant marginal bone loss.

as induce an excessive static force when an attempt is made to secure the framework to the implants.³⁰ Therefore, implant framework misfit could be a contributing factor to peri-implant bone loss and/or implant failure; however, findings from current literature have been controversial.^{25,29,31}

Implant stability decreases during the first 4 weeks following implant placement before rebounding, as measured by resonance frequency analysis.^{32,33} This may result in a short time

period during which implants are more likely to move slightly under load. It has also been shown that deformations of the implant framework and the surrounding bone can occur when tightening a vertically misfit implant framework.^{30,34} Jemt and Lekholm reported a mean framework displacement of 177 μm (range: 100–300 μm) and a mean implant displacement of 123 μm (range: 60–200 μm) when an implant framework with approximately 1 mm vertical misfit was tightened to implants that had been osseointegrated under a mean preload of 246 N (mean torque: 25.9 Ncm).³⁰ This corresponded to a mean 300 μm (30%) total gap closure; however, immediately loaded implants may be able to further close a prosthetic misfit gap, as compared to integrated implants. When comparing gap closure under a 35 Ncm torque in ~ 500 μm vertically misfit frameworks on the statically immediately loaded and healed implants, Duyck *et al* observed a mean gap closure of 71% and 39%, respectively.³⁴ They attributed this phenomenon principally to the implant movement caused by bone deformation, owing to strain and microfracture.³⁴ Interestingly, all immediately loaded implants were in contact with the prostheses at some point, but the gaps were not closed completely due to additional horizontal discrepancies between implant and prosthesis cylinder inclination.³⁴

In this report, the provisional framework misfits noted immediately after implant placement seemed to be completely closed after being repeatedly hand-tightened over a 2-week period. This suggests that in addition to the apparent adaptation of vertical discrepancies, hand-tightening force may also

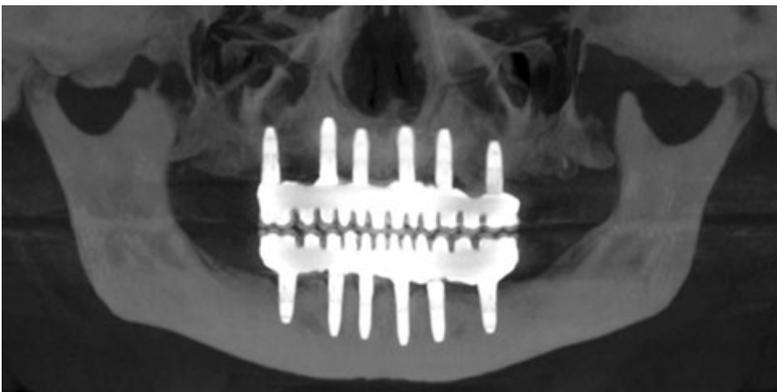


Figure 6 CBCT image of the final prosthesis 3 years after the surgery. Despite initial peri-implant marginal bone loss, the bone levels had been well maintained since 6 months after the surgery.

allow for adaptation of horizontal and angular discrepancies, if minimal enough. Furthermore, it is possible that the initial framework displacement by hand-tightening would be greater with an acrylic than a metal framework due to the former's lower modulus of elasticity; however, the resulting implant adaptation to the strain of a misfit acrylic prosthesis compared to one with a metal framework is unknown.

Both aforementioned studies^{30,34} also concluded that static forces induced by prosthesis misfit did not lead to biologic failure of the already osseointegrated or statically immediately loaded implants. While an $\sim 700 \mu\text{m}$ mean crestal bone loss was observed in the latter study, this is not beyond the expected observed peri-implant marginal bone loss values.³⁵ However, a study that investigated the influence of static and dynamic implant loading has shown that less bone density and crater-like bone defects lateral to osseointegrated implants were observed with excessive dynamic loads.³⁶ Granted, these studies were conducted in the rabbit tibia and not in the human oral cavity where other factors such as intraoral microflora and oral hygiene might have affected the outcome. In the patient situation presented, a significant mean marginal bone loss of 2.1 mm (range: 1.4 to 3.5 mm) was observed 6 months after the implant surgery and interim prostheses placement (Fig 5). Since this value is considerably higher than mean bone loss reported in immediately loaded implants supporting FCDs, with (0.6 to 0.9 mm)^{37,38} or without (1.2 to 1.6 mm)^{39,40} flap reflection, a combination of framework misfit (static load) and immediately loaded implants (dynamic load) might contribute to the substantially excessive loads that lead to such significant bone loss; however, at 3 years, all implants remained osseointegrated, and minimal further marginal bone level change was observed, suggesting that unfavorable conditions had been reversed, and equilibrium had been reached (Fig 6).

Conclusions

Prosthetic misfit can occur during computer-guided implant placement and the immediate provisionalization procedure, especially when multiple implants are involved. In this report, biologic adaptation of immediately loaded implants under static force seems to be responsible for the misfit correction; however, a combination of framework misfit (static load) and immediately loaded implants (dynamic load) might contribute to the substantially excessive loads that lead to significant bone loss. Therefore, it is recommended that framework misfit be avoided or corrected in immediate loading situations. Nevertheless, it should be noted that this is an individual clinical report, and the outcome should not be generalized. Further studies related to prosthetic misfit and biological adaptation are needed to substantiate or refute the finding of this clinical report.

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