ORIGINAL ARTICLE

Y. Wu J. Kuo G. J. Wright S. E. Cisewski F. Wei M. J. Kern H. Yao

Viscoelastic shear properties of porcine temporomandibular joint disc

Authors' affiliations:

Y. Wu, J. Kuo, G. J. Wright, S. E. Cisewski,
F. Wei, H. Yao, Department of Bioengineering, Clemson University, Clemson,
SC, USA
M. J. Kern, H. Yao, Department of Oral Health Sciences, Medical University of

South Carolina (MUSC), Charleston, SC, USA

Correspondence to:

H. Yao, PhD Department of Bioengineering Clemson University Clemson-MUSC Bioengineering Program 68 President Street MSC 501 Charleston, SC 29425 USA E-mail: haiyao@clemson.edu

Date:

Accepted 24 November 2014

DOI: 10.1111/ocr.12088

© 2015 John Wiley & Sons A/S. Published by John Wiley & Sons Ltd Wu Y., Kuo J., Wright G. J., Cisewski S. E., Wei F., Kern M. J., Yao H. Viscoelastic shear properties of porcine temporomandibular joint disc *Orthod Craniofac Res* 2015; **18**(Suppl.1): 156–163. © 2015 John Wiley & Sons A/S. Published by John Wiley & Sons Ltd

Structured Abstract

Objectives – To investigate the intrinsic viscoelastic shear properties in porcine TMJ discs.

Materials and methods - Twelve fresh porcine TMJ discs from young adult pigs (6-8 months) were used. Cylindrical samples (5 mm diameter) with uniform thickness (~1.2 mm) were prepared from five regions of the TMJ disc. Torsional shear tests were performed under 10% compressive strain. Dynamic shear was applied in two methods: 1) a frequency sweep test over the frequency range of 0.1-10 rad/s with a constant shear strain amplitude of 0.05 rad and 2) a strain sweep test over the range of 0.005-0.15 rad at a constant frequency of 10 rad/s. Transient stress relaxation tests were also performed to determine the equilibrium shear properties. Results - As the frequency increased in the frequency sweep test, the dynamic shear complex modulus increased, with values ranging from 7 to 17 kPa. The phase angle, ranging from 11 to 15 degrees, displayed no pattern of regional variation as the frequency increased. The dynamic shear modulus decreased as the shear strain increased. The equilibrium shear modulus had values ranging from 2.6 to 4 kPa. The posterior region had significantly higher values for dynamic shear modulus than those in the anterior region, while no significant regional difference was found for equilibrium shear modulus.

Conclusion – Our results suggest that the intrinsic region-dependent viscoelastic shear characteristics of TMJ disc may play a crucial role in determining the local strain of the TMJ disc under mechanical loading.

Key words: dynamic mechanical testing; porcine animal model; shear modulus; temporomandibular joint disc



Introduction

Temporomandibular disorders (TMD) resulting in pain and disability are the second most common musculoskeletal condition, affecting 5-12% of the population with healthcare and societal costs of \$4 billion in the United States (1). Temporomandibular joint (TMJ) disc dysfunction and associated pain occur in approximately 30% of patients with TMD (2, 3). The primary function of the TMJ disc is to provide mechanical support and prevent bone to bone contacts that can result in significant damage and loss of joint function. Nickel et al. (4) has suggested that synovial fluid may reduce friction, but abnormal loading as a result of clenching or grinding can reduce the fluid boundary resulting in direct cartilage contacts. Sustained mechanical loading can cause decreases in fluid load support and increased friction that may result in excessive tissue shear stress and wear (5). Studies have found that dynamic shear stress or excessive shear strain can result in fatigue and/or failure of the TMJ disc (6-10). Pathological loading may also cause permanent collagen damage and cartilage degradation that can result in the development of osteoarthritis (11, 12). However, the mechanism through which the mechanical loading initiates pathological events within the TMJ disc is still poorly understood. One requirement for studying TMJ pathology and development of tissue engineered treatments is the characterization of disc mechanical properties and the resulting biological responses. These properties will be crucial in determining a suitable animal model as well as for building a predictive model of TMJ disorders.

Previously, the compression and tensile properties of the TMJ disc were characterized to better understand the complex function and environment in the cartilage tissue (13–18). During jaw motion, the fossa remains stationary while the condyle bone articulates. As a result, the sandwiched TMJ disc is also subjected to the shear force as well as a variety of compressive and tensile forces. Furthermore, due to the incongruities between the bone and cartilage surfaces, non-uniform deformation of the disc will result in the development of local shear stress. Another potential cause of shear stresses is the variation of extracellular matrix (ECM) structure and distribution across the disc. Collagen fibres have a ring-like alignment along the disc periphery and run anteroposteriorly through the central region of the disc (19). Due to the low glycosaminoglycan (GAG) content of TMJ discs, shear properties are largely believed to be associated with the collagen content and orientation. Previous studies have shown that excessive shear stress can result in fatigue and permanent damage of the TMJ disc (6-9). However, the static/equilibrium and dynamic shear properties have not been fully examined in relation to varying frequency, strain and disc region.

Previous studies have shown that the shear modulus of TMJ discs was largely dependent on frequency and direction of loading, which may be a result of region-dependent biochemical composition (20). It is generally believed that tensile loads occurring within the cartilage are a result of shear and friction produced during joint motion (21). Studies have found that the viscoelasticity of the disc during tension and shear, unlike compression, is largely flow independent and primarily supported by the solid phase (22). These findings highlighted the importance of testing within a reasonable frequency (~0.5-2 Hz during chewing) and under sufficient compressive loading (10% strain during clenching) to maintain a physiological basis.

Using rotational shear experiments, the region-dependent equilibrium modulus and dynamic viscoelastic properties of porcine TMJ discs were examined in this study. Due to the inhomogeneous and viscoelastic nature of the disc, the shear properties were examined in relation to frequency and shear strain in five disc regions. It has been showed that the porcine model is an acceptable analogue for human samples (23–26). Therefore, the goal of this study was to determine viscoelastic shear properties of the porcine TMJ disc model and how these relate to TMJ disc structure and function. The hypothesis of this study is that mechanical shear properties of TMJ discs are viscoelastic and region-dependent.

Materials and methods Sample preparation

Twelve TMJ discs from the left joint were harvested from pig heads (6-8 month old, Yorkshire, male) obtained from a local slaughterhouse within 2 h of sacrifice. Sample size is based on the error analysis of our previous works on viscoelastic properties of human TMJ discs under confined compression (18). The discs were immediately photographed, morphologically examined and wrapped in gauze soaked in a normal saline solution with protease inhibitors and stored at -80°C until mechanical testing. It has been reported that mechanical properties of porcine discs were retained over five freeze-thaw cycles (27). Discs exhibiting any abnormalities (i.e. fissures or bruising) were discarded.

Cylindrical tissue plugs were obtained from the anterior, intermediate, lateral, medial and posterior regions of the TMJ disc (Fig. 1A), using a 5-mm corneal trephine (Biomedical Research



Fig. 1. (A) Schematic of specimen preparation. The region and size of test specimens are shown. Shear samples from the five disc regions had an average height of 1.0 mm and a diameter of 5 mm. (B) Schematic of rotational shear chamber.

Instruments Inc., Silver Spring, MD, USA). Thin layers from the superior and inferior surfaces were removed via a sledge microtome (Model SM2400; Leica Instruments, Nussloch, Germany) with a freezing stage (Model BFS-30; Physitemp Instruments Inc., Clifton, NJ, USA) to eliminate the natural concave shape of the disc and allow for a flat surface during mechanical testing. Shear samples had an average height of 1.0 mm and a diameter of 5 mm.

Testing configuration

Cylindrical tissue samples were placed in custom designed shear chamber that allowed for complete immersion in PBS to prevent dehydration (Fig. 1B). Prior to testing, 200 grit sandpaper was affixed to both surfaces of the stainless steel 8-mm parallel plate geometry with cyanoacrylate glue. This was necessary to prevent sample slipping during high-frequency rotations. The sandpaper was allowed to soak in PBS prior to zeroing of the gap to prevent errors in the measurement of sample height.

Rotational shear experiments were performed with a TA Instruments AR G2 (New Castle, DE, USA) at 37°C maintained by a water-cooled Peltier plate. The instrument has a displacement resolution of 25 nrad and a torque resolution of 0.1 nN/m. Initial height was measured by lowering the probe onto the sample and recording the height occurring at 5 mN of force. Samples were then compressed 10% of the initial measured height to ensure full contact of the surface and prevent slipping during rotation. Studies have suggested that this amount of strain corresponds to a loaded joint (28).

Loading protocol

Three testing protocols were used to measure the static and dynamic viscoelastic properties of the disc. These included a frequency sweep, strain sweep and a stress relaxation test (Fig. 2). The frequency sweep was over a range of 0.1– 10 rad/s (0.016–1.59 Hz) at a constant angular strain of 0.05 radians (~2.86°; angle in degrees = angle in radians \times 180°/ π). The strain



Fig. 2. Loading protocols of frequency sweep, strain sweep and stress relaxation experiments. γ_0 represents initial amplitude of the shear strain.

sweep was over a strain range of 0.005–0.15 radians (~0.29°–8.6°) at an angular frequency of 10 rad/s. The stress relaxation occurred in strain steps of 0.05 radian increases from 0.005 to 0.15 radians with each level maintained for 900 s to measure the equilibrium shear modulus. In this study, small shear strains were used to measure the flow independent material properties. Complex modulus and phase angle were recorded for dynamic experiments. Equilibrium shear modulus was calculated from the slope of the equilibrium stress vs. strain curve generated from all five stress relaxation steps.

Statistical analysis

The shear properties were examined for significant differences between disc regions using SPSS statistics software (SPSS 21.0; IBM, Armonk, NY, USA). One-way ANOVA and Tukey's *post hoc* tests were performed to determine whether significant differences existed. Statistical differences were reported at *p*-values <0.05.

Results Frequency sweep

In the shear frequency sweep experiments, the magnitude of the complex modulus $|G^*|$ and phase angle was significantly frequency dependent (Fig. 3). Complex modulus values for the posterior region were significantly higher than those in the anterior region over the entire frequency range (p = 0.025). Average standard deviations for complex moduli were approximately

45% of average moduli values (not shown in the figure). At a frequency of 6.28 rad/s (~1 Hz), the average $|G^*|$ of the central region was 11.22 ± 5.2 kPa, 10.20 ± 4.9 kPa for the anterior, and 15.38 ± 6.07 kPa for the posterior region. Phase angle decreased with increasing frequency



Fig. 3. Shear frequency sweep of porcine TMJ discs. (A) Relationship of complex modulus with frequency. (B) Relationship of phase angle with frequency.

until 1 rad/s was reached then began to increase with increasing frequency. Phase angle values only varied between 11° and 15° and showed no regional variation. Average phase angle standard deviations were approximately 15% of measured phase angles (not shown in figure).

Strain sweep

In the strain sweep experiments, the complex modulus significantly decreased with increasing rotational strains (Fig. 4). The posterior region once again was significantly higher than anterior and medial regions for $|G^*|$ over all strains tested (p = 0.018). Average standard deviations were 40% of the magnitude of complex modulus values (not shown in the figure). Although phase



Fig. 4. Shear strain sweep of porcine TMJ discs. (A) Relationship of complex modulus with shear strain. (B) Relationship of phase angle with shear strain.

160 Orthod Craniofac Res 2015;18(Suppl.1):156–163

angle increased with increasing strain for all regions, it only varied between 11° and 15° and showed no significant regional variation. Average phase angle standard deviations were 15% of measured values (not shown in figure).

Equilibrium shear modulus

The rotational shear equilibrium modulus was measured by performing stepwise stress relaxations at increasing strain steps (Fig. 5). The slope of the resulting stress vs. strain curve at equilibrium was used to calculate the modulus. Although no significant regional variation was detected, the posterior region had the highest average modulus value and the anterior had lowest average modulus value (posterior: 3.88 ± 1.76 kPa; anterior: 2.57 ± 1.61 kPa). The overall average equilibrium modulus across the disc was 3.53 ± 1.61 kPa.

Discussion

The objective of this study was to determine the viscoelastic shear properties of the porcine TMJ disc model and how these relate to TMJ disc structure and function. The results demonstrated that the viscoelastic shear properties are dependent on region, loading frequency and strain. Lai et al. investigated the static shear properties of human TMJ discs and found the shear moduli of the peripheral regions to be significantly higher than those in the central portions. In our study, the posterior region exhibited significantly higher complex moduli for frequency and strain sweeps as well as a relatively higher average equilibrium modulus. By contrast, the anterior region showed relatively lower moduli for all of the experiments. This unique regional difference could be explained by the inhomogeneous collagen fibre structure and biochemical components in the porcine TMJ disc, which were shown in our previous conductivity and fluorescence recovery after photobleaching (FRAP) studies (29, 30). The scanning electron microscope (SEM) study also further confirmed that collagen fibre structure in the anterior region is more isotropic with a significantly lower coherency



Fig. 5. (A) Typical stress relaxation curve for disc sample from anterior region. The multistrain levels included five steps (0.005, 0.01, 0.05, 0.1 and 0.15). As shown in the inset plot, the shear equilibrium modulus was calculated from the slope of equilibrium stress vs. strain curve generated from all five stress relaxation steps. (B) Average \pm standard deviation of regional shear equilibrium modulus.

coefficient than the other regions in the disc (30).

The relationship of dynamic shear properties with the frequency and strain in the TMJ disc is consistent with results found in bovine meniscus and human annulus fibrosus (AF) (7, 31). Previous studies also found the tensile and shear properties of TMJ discs to be largely fluid flow independent suggesting much greater load support from the solid phase of the tissue (22). These findings were further supported with the results of our dynamic frequency and strain sweeps. Phase angles only varied between 11° and 15° that was a significantly smaller range than observed during dynamic compression experiments in our previous study (~ $15^{\circ}-30^{\circ}$). By contrast, dynamic shear modulus values were found to be significantly lower than confined compression dynamic modulus values (18). Furthermore, the phase angle was found to be increased, while the complex modulus was decreased under larger shear strain levels. All of these findings suggest that during small rotational strain experiments, the solid phase of the tissue behaves elastically and the flow-dependent effect was isolated from the flow independent viscoelasticity (31). Therefore, the shear modulus measured in this study represents the intrinsic viscoelasticity in the TMJ disc.

Very few studies have characterized the viscoelastic properties of the human TMJ disc which may be due to difficulty in obtaining samples (32, 33). Many studies have characterized the compressive, tensile and shear mechanical properties of a variety of animal species. Several groups concluded that the pig is the best experimental model of the TMJ after comparison to sheep, cows, dogs, cats, rabbits, rats and goats (24, 26). In particular, selection of the pig was attributed to the similar size of TMJ structures, shape of the disc and omnivorous diet. In addition, the pig and human TMJs have been shown to have similar gross morphology and structure, including the disc and its attachments. Moreover, both pig and human TMJs have a similar range of motion (23, 25). While all these reasons served as the rationale for using porcine TMJ discs in this study, it is necessary to measure the viscoelastic shear properties of human TMJ discs in a future study.

Lai's study also found significant increases in shear moduli with increasing age suggesting changes in morphology over time. The average shear modulus measured in the Lai study ranged between 1 and 1.75 MPa that was several hundred times greater than the values measured in this study (~3 kPa). These significant differences are likely a result of testing configuration differences. In the Lai study, samples were loaded with parallel shear plates and tested to failure, which suggests forces much higher than those experienced *in vivo* (34). Tissue samples were attached to the testing apparatus with adhesive which could infiltrate the tissue and alter the viscoelastic properties measured. Furthermore, compared with the human AF, which was measured with a similar torsional shear testing configuration (31), the shear modulus in this study is relatively smaller but still in the same kPa magnitude (this study: 5-25 kPa; human AF: 20-150 kPa). Larger values in human AF tissue could be due to the difference of normal stresses applied to the samples (TMJ discs in this study: 2.5-7.4 kPa for 10% strain compression; human AF: 17.5-35 kPa due to directly compressive loading). Previous studies also indicated that the dynamic properties of the TMJ disc are affected by the temperature-sensitive collagen and proteoglycan components. A higher temperature (body temperature instead of room temperature) may reduce the stiffness and strength of the disc (8, 14, 35). In addition, the sample preparation method used in this study also has its limitations. Bone trephine punching and microtome cutting could alter the ECM collagen structure by reducing the intrinsic tension of the collagen fibre and weaken its sustainability against shear force.

Conclusions

In conclusion, this study shows that the porcine TMJ disc has frequency and strain-dependent inhomogeneous shear properties, which are similar to that in the human TMJ disc. It helps to further understand the role of mechanical loading on TMJ daily function and the pathological mechanism of TMJ disorders. Furthermore, it also provides essential mechanical parameters for further finite element analysis on TMJ kinematics and mechanics for early diagnosis or function assessment.

Clinical relevance

The National Institute of Dental and Craniofacial Research (NIDCR) reports that TMJ disorders resulting in pain and disability are the second most common musculoskeletal condition, affecting 5-12% of the population with annual healthcare costs of \$4 billion. Mechanical dysfunction of the TMJ disc, especially displacement due to tissue degeneration, is central to many TMJ disorders. It is generally believed that pathological mechanical loadings, for example sustained jaw clenching or malocclusion, trigger a cascade of molecular events leading to TMJ disc degeneration. Therefore, characterization of disc mechanical properties is essential to help understand the pathological mechanism and provide guidelines for disc tissue regeneration.

Acknowledgements: This project was supported by NIH Grants DE018741, DE021134 and AR055775, a NIH F31 training Grant DE020230 to JK, and a NIH F31 training Grant DE023482 to GJW.

References

- 1. Stowell AW, Gatchel RJ, Wildenstein L. Cost-effectiveness of treatments for temporomandibular disorders: biopsychosocial intervention versus treatment as usual. *J Am Dent Assoc* 2007;138:202–8.
- 2. Ahmad M, Hollender L, Anderson Q, Kartha K, Ohrbach R, Truelove EL et al. Research diagnostic criteria for temporomandibular disorders (RDC/TMD): development of image analysis criteria and examiner reliability for image analysis. *Oral Surg Oral Med Oral Pathol Oral Radiol Endod* 2009;107:844–60.
- 3. Schiffman EL, Truelove EL, Ohrbach R, Anderson GC, John MT, List T

et al. The Research Diagnostic Criteria for Temporomandibular Disorders. I: overview and methodology for assessment of validity. *J Orofac Pain* 2010;24:7–24.

- 4. Nickel JC, McLachlan KR. In vitro measurement of the stress-distribution properties of the pig temporomandibular joint disc. *Arch Oral Biol* 1994;39:439–48.
- Park S, Krishnan R, Nicoll SB, Ateshian GA. Cartilage interstitial fluid load support in unconfined compression. *J Biomech* 2003;36:1785–96.
- Zhu W, Mow VC, Koob TJ, Eyre DR. Viscoelastic shear properties of articular cartilage and the effects

of glycosidase treatments. J Orthop Res 1993;11:771–81.

- Zhu W, Chern KY, Mow VC. Anisotropic viscoelastic shear properties of bovine meniscus. *Clin Orthop Relat Res* 1994;306:34–45.
- Tanaka E, van Eijden T. Biomechanical behavior of the temporomandibular joint disc. *Crit Rev Oral Biol Med* 2003;14:138–50.
- Spirt AA, Mak AF, Wassell RP. Nonlinear viscoelastic properties of articular cartilage in shear. *J Orthop Res* 1989;7:43–9.
- Gallo LM, Nickel JC, Iwasaki LR, Palla S. Stress-field translation in the healthy human temporomandibular joint. J Dent Res 2000;79:1740–6.

- 11. Tanaka E, Rego EB, Iwabuchi Y, Inubushi T, Koolstra JH, van Eijden TM et al. Biomechanical response of condylar cartilage-on-bone to dynamic shear. *J Biomed Mater Res* 2008;85:127–32.
- Zarb GA, Carlsson GE. Temporomandibular disorders: osteoarthritis. *J Orofac Pain* 1999;13:295–306.
- Beatty MW, Nickel JC, Iwasaki LR, Leiker M. Mechanical response of the porcine temporomandibular joint disc to an impact event and repeated tensile loading. *J Orofac Pain* 2003;17:160–6.
- Detamore MS, Athanasiou KA. Tensile properties of the porcine temporomandibular joint disc. *J Biomech Eng* 2003;125:558–65.
- Lomakin J, Sprouse PA, Detamore MS, Gehrke SH. Effect of pre-stress on the dynamic tensile behavior of the TMJ disc. *J Biomech Eng* 2014; 136:011001.
- Snider GR, Lomakin J, Singh M, Gehrke SH, Detamore MS. Regional dynamic tensile properties of the TMJ disc. J Dent Res 2008;87:1053–7.
- 17. Willard VP, Kalpakci KN, Reimer AJ, Athanasiou KA. The regional contribution of glycosaminoglycans to temporomandibular joint disc compressive properties. *J Biomech Eng* 2012;134:011011.
- Kuo J, Zhang L, Bacro T, Yao H. The region-dependent biphasic viscoelastic properties of human temporomandibular joint discs under confined compression. *J Biomech* 2010;43:1316–21.
- Allen KD, Athanasiou KA. Tissue engineering of the TMJ disc: a review. *Tissue Eng* 2006;12:1183–96.

- 20. Tanaka E, Hanaoka K, van Eijden T, Tanaka M, Watanabe M, Nishi M et al. Dynamic shear properties of the temporomandibular joint disc. *J Dent Res* 2003;82:228–31.
- 21. Singh M, Detamore MS. Biomechanical properties of the mandibular condylar cartilage and their relevance to the TMJ disc. *J Biomech* 2009;42:405–17.
- 22. Huang CY, Mow VC, Ateshian GA. The role of flow-independent viscoelasticity in the biphasic tensile and compressive responses of articular cartilage. *J Biomech Eng* 2001;123: 410–7.
- 23. Herring SW, Decker JD, Liu ZJ, Ma T. Temporomandibular joint in miniature pigs: anatomy, cell replication, and relation to loading. *Anat Rec* 2002;266:152–66.
- 24. Kalpakci KN, Willard VP, Wong ME, Athanasiou KA. An interspecies comparison of the temporomandibular joint disc. *J Dent Res* 2011;90:193–8.
- Mills DK, Daniel JC, Herzog S, Scapino RP. An animal model for studying mechanisms in human temporomandibular joint disc derangement. J Oral Maxillofac Surg 1994;52:1279–92.
- Stembirek J, Kyllar M, Putnova I, Stehlik L, Buchtova M. The pig as an experimental model for clinical craniofacial research. *Lab Anim* 2012;46:269–79.
- 27. Allen KD, Athanasiou KA. A surfaceregional and freeze-thaw characterization of the porcine temporomandibular joint disc. *Ann Biomed Eng* 2005;33:951–62.
- 28. Tanaka E, Iwabuchi Y, Rego EB, Koolstra JH, Yamano E, Hasegawa

T et al. Dynamic shear behavior of mandibular condylar cartilage is dependent on testing direction. *J Biomech* 2008;41:1119–23.

- Kuo J, Wright GJ, Bach DE, Slate EH, Yao H. Effect of mechanical loading on electrical conductivity in porcine TMJ discs. *J Dent Res* 2011;90:1216– 20.
- 30. Shi C, Wright GJ, Ex-Lubeskie CL, Bradshaw AD, Yao H. Relationship between anisotropic diffusion properties and tissue morphology in porcine TMJ disc. Osteoarthritis Cartilage 2013;21:625–33.
- Iatridis JC, Kumar S, Foster RJ, Weidenbaum M, Mow VC. Shear mechanical properties of human lumbar annulus fibrosus. J Orthop Res 1999;17:732–7.
- 32. Beek M, Aarnts MP, Koolstra JH, Feilzer AJ, van Eijden TM. Dynamic properties of the human temporomandibular joint disc. *J Dent Res* 2001;80:876–80.
- 33. Tanaka E, Shibaguchi T, Tanaka M, Tanne K. Viscoelastic properties of the human temporomandibular joint disc in patients with internal derangement. J Oral Maxillofac Surg 2000;58:997–1002.
- Lai WF, Bowley J, Burch JG. Evaluation of shear stress of the human temporomandibular joint disc. *J* Orofac Pain 1998;12:153–9.
- 35. Tanaka E, Aoyama J, Tanaka M, Van Eijden T, Sugiyama M, Hanaoka K et al. The proteoglycan contents of the temporomandibular joint disc influence its dynamic viscoelastic properties. *J Biomed Mater Res* 2003;65:386–92.

Copyright of Orthodontics & Craniofacial Research is the property of Wiley-Blackwell and its content may not be copied or emailed to multiple sites or posted to a listserv without the copyright holder's express written permission. However, users may print, download, or email articles for individual use.